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## Color characteristics of various computerized machinable ceramics veneered to Yttria-Stabilized Tetragonal Zirconia Polycrystalline Upon different hybridized techniques

Niwut Juntavee <sup>1</sup>, Apa Juntavee <sup>2</sup>, Siripim Tangsatchatham <sup>3</sup><sup>1</sup> Department of Prosthodontics, Faculty of Dentistry, Khon Kaen University, Khon Kaen, Thailand<sup>2</sup> Division of Pediatric Dentistry, Department of Preventive Dentistry, Faculty of Dentistry, Khon Kaen University, Khon Kaen, Thailand<sup>3</sup> Division of Biomaterials and Prosthodontics, Faculty of Dentistry, Khon Kaen University, Khon Kaen, Thailand**Correspondence:**

Niwut Juntavee

Department of Prosthodontics

Faculty of Dentistry, Khon Kaen University

Khon Kaen, Thailand

niwutpapa@hotmail.com

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**Abstract**

**Background:** Hybridization technique impacted color of ceramic veneered zirconia. This study examined color characteristics of different ceramics veneered zirconia upon different hybridized techniques.

**Material and Methods:** 120 zirconia specimens (0.8 mm thickness, 12 mm diameter) were prepared from 3-yttria-stabilized tetragonal zirconia polycrystalline and unintentionally veneered with Vitabloc Mark-II (Vm), IPS e.max CAD (Em), Vita-Suprinity (Vs), and Celtra-Duo (Cd), by CAD-bonded (Cb) versus CAD-fused (Cf) hybridization (n=15/group). CIE-L\*a\*b\* color characteristics were determined for translucency parameter (TP), contrast ratio (CR), opalescence parameter (OP), and color difference ( $\Delta E_{diff}$ ). Microstructures were investigated with SEM and XRD. Analysis of Variance and Bonferroni comparisons were determined for significant differences ( $p < 0.05$ ). **Results:** TP and OP were significantly higher, but lower CR and  $\Delta E_{diff}$  for Vm and Em than Cd and VS. Cf hybridized technique significantly decreased TP and OP but increased CR and  $\Delta E_{diff}$  than Cb, which amplified color alteration. Better TP and OP, with less CR and  $\Delta E_{diff}$  were achieved for zirconia veneering with either Vm or Em, compared to Vs or Cd, whether hybridized with Cb or Cf technique.

**Conclusions:** Different veneering ceramics and hybridized techniques significantly altered color characteristics of ceramic veneered zirconia. Zirconia veneering with either Vm or Em appeared to produce better translucence and opalescence, with less contrast and color alteration than veneering with either Vs or Cd. CAD-fused decreased translucency, opalescence, and intensified color alteration due to t→m transformation. Nevertheless, the color alteration of ceramics veneered zirconia still rendered an acceptable limit, except for both Vs and Cd upon Cf hybridization.

**Key words:** CAD/CAM, color, contrast, hybridized technique, opalescence, translucency.

## Introduction

The progression in the technological elaboration of computer-aided design-computer-aided manufacturing (CAD/CAM) has become an increasingly useful technique for contemporary practice in dentistry (1). The evolution of this technology and the increasing demand for esthetics in dentistry commenced the dental practitioner and dental researcher to search for new ceramic materials that can render high-quality and reliable esthetic reconstruction (2). Amongst recently progressed ceramic materials, stabilized zirconia has gained increasing attractiveness as an exceptional replacement to metal owing to its auspicious aesthetics, biological compatibility, insignificant bacterial plaque accumulation together with optimal strength, and prime fracture toughness (3). Zirconia encompassed three microstructural phases: monoclinic (m-), tetragonal (t-), and cubic (c-) phases. These phases are interchangeable due to the triggered temperature. At the ambient temperature, the m-phase was detectable. Upon heating up to 1,170°C, the m-phase was induced to transform to the t-phase until the temperature reached 2,370°C, and the c-phase appeared and remained unchanged up to the melting point of 2,680°C. As cooling down, all the microstructures turn into the m-phase (4). To achieve and stabilize the desired t-phases at room temperature, a yttrium oxide stabilizer ( $Y_2O_3$ ) was added. The 3 mol%  $Y_2O_3$  was implemented into zirconia as called 3 mol% yttria-stabilized tetragonal polycrystalline (3Y-TZP) and presented almost the entire t-phase at the normal temperature. The superior advantages of 3Y-TZP restoration to endure the force of mastication founded on the metaphysical phase transitions from the t→m-phase as induced by external stimuli such as moisture, stress, and warmth, causing 4–5% volumetric expansion that enables stabilized zirconia as an exceptional strength called “transformation toughening” to prevent crack propagation and enhance strength for extensive restoration (4). However, zirconia is noticeably opaque white with a relatively high refractive index and diminishes light transmission (5,6). It essentially needs veneering ceramic to ensure aesthetic outcomes (7,8). The mechanical and optical properties allowed 3Y-TZP to be used as a substructure for veneering with translucent ceramic to render aesthetic restorations (5-7,9).

Traditional ceramic layering techniques have been used as the most typical technique in ceramic veneering zirconia. Several reports stated that ceramic veneered zirconia restorations predominantly deteriorated from cracking and delamination of the veneering ceramic up to 15-36% in 5 years of the follow-up period, which is the most commonly reported clinical complication (4,10). Although an exclusive prominent monolithic translucent 3Y-TZP has been introduced for the construction of absolute solid restorations to avoid chipping and de-

lamination of veneering ceramic, its' translucency still does not reach the desirable achievement (9). Hence, this circumstance restricts its usage as full-contoured restoration barely in the posterior region of the arch, yet it is still primarily used as a substructure for veneering with feldspathic or glass-ceramic (3). Alteration of the firing protocol has resulted in greater resistance to fracture of the ceramic veneered zirconia restorations (11). Other approaches have been established to increase the clinical implementation of ceramic veneered zirconia including the pressed-on ceramic veneering zirconia which is a technique for veneering zirconia by pressing procedure (12). However, the clinical outcome is still not fully satisfied and technique sensitive. The most recent strategy includes that both zirconia substructure and veneering ceramic are CAD/CAM generated which results in highly predictable outcomes since the ceramic blanks are industrially produced with improved reliability and quality control (13). Several modern ceramics for CAD/CAM were introduced for this technique. For instance, lithium disilicate (LS2) glass-ceramic was proposed to enhance the mechanical property of feldspathic ceramic and it has been recommended as an alternative veneering ceramic for zirconia (13). More recently, zirconia-reinforced lithium silicate (ZLS) has been introduced as a new ceramic material proposed for CAD/CAM restoration. This syndicates the optimistic mechanical advantages of the zirconia with the esthetic appearance of glass ceramic, providing higher mechanical properties compared to LS2 glass ceramic (2,14). After the zirconia substructure and the veneering ceramic were CAD/CAM generated, both components were hybridized together by fusing with low fusion glass under appropriate sintering temperature (CAD-fused, Cf) or by bonding with resin cement (CAD-bonded, Cb). The Cf hybridized technique can produce a homogeneous multilayered restoration without initiating flaws or defective structures. While the Cb hybridized technique is more appropriate for an extensive reconstruction that does not need to be sintered, thereby, avoiding distortion from the sintering process (13).

The esthetic outcomes of ceramic veneered zirconia are influenced by types of veneering ceramic and their hybridized techniques (15,16). Veneering ceramic can enhance esthetic restoration by improving color characteristics of restorations in terms of translucency, contrast, opalescence, and color predictability (17,18). Translucence was defined by the quantity of light transmission across a material, which was identified as an existing condition between total opacity and transparency, and can be signified by the translucency parameter (TP) as well as contrast ratio (CR) (6,19). The material with superior translucence would permit greater light transmission and exhibited a greater TP but lesser CR values because both parameters are adversely associated. The

crystalline structures, grain sizes, colorant mixtures, and porosities were stated to disturb the trajectory of light (20). The restoration should look blueish once the light is reflected out of it and emerge an orange manifestation once the light diffuses through the material. This occurrence is recognized as “opalescence”, signified by the opalescence parameter (OP), and attentively simulated appearance of human enamel (21,22). The supreme concern for dentists in providing aesthetic restoration for the patient is how to get the restoration fabricated by a dental technician with predictable color as prescribed. Likewise, the dental technician is often frustrated with how to fabricate the restoration based on the material and existing technique to meet the dentist’s demand. Thus, different types of materials and techniques used for fabrication should produce the color appearance of restoration within an acceptable color perception (23). The color difference ( $\Delta E_{\text{diff}}$ ) was employed to verify the level of perception, which was determined by the perceptibility threshold (PT,  $\Delta E_{\text{diff}} = 2.6$ ) and acceptability threshold (AT,  $\Delta E_{\text{diff}} = 5.5$ ). It indicated “clinically indistinguishable” as  $\Delta E_{\text{diff}} \leq 2.6$ , “clinically acceptable” as  $\Delta E_{\text{diff}} = 2.6-5.5$ , and “clinically unacceptable” as  $\Delta E_{\text{diff}} > 5.5$  (24).

Whilst computerized machinable ceramics veneered to zirconia upon hybridized techniques is a fairly new method, a lack of evidence regarding the color characteristics upon the hybridized techniques of contemporary machinable ceramics veneered zirconia substructure. Currently, LS2 ceramics is the only material intended to be connected with a zirconia substructure using fusion glass, other CAD/CAM-manufactured glass ceramics have never been used with this method (7,13). Moreover, previous studies commonly determined color perception by human judgment which restricted the capability to distinguish minute color differences and seem subjectively compared (1,6,10). To avoid non-reproducibility, color determination should be performed with a quantitative spectrophotometer (1). As such, the objective of this study was to evaluate the effect of different veneering ceramics and hybridized techniques on color characteristics of CAD/CAM fabricated ceramic veneered zirconia, including translucency, contrast, opalescence, and color alteration. The null hypothesis was that there was no significant difference in TP, CR, OP, and  $\Delta E_{\text{diff}}$  of CAD/CAM generated ceramic veneering zirconia upon using different ceramics veneering, hybridization techniques, and these interactions.

## Material and Methods

This experimental study determined the sample size from the statistical data performed by Sailer and colleagues’ publication in 2007 (25) using G\*power software version 3.1 (Heinrich Heine University, Düsseldorf, Germany) with a power of test = 0.90 and  $\alpha$  error = 0.05 as shown in Equation 1, (Fig. 1).

$$N \text{ per group} = \frac{(Z_{\alpha/2} + Z_{\beta})^2 (s_1^2 + s_2^2)}{(\mu_1 - \mu_2)^2}$$

Fig. 1: Equation 1.

Which:  $Z_{\beta}$  = standard normal deviation = 1.28 ( $\beta$  error = 0.1),  $Z_{\alpha}$  = standard normal deviation = 1.96 ( $\alpha$  error = 0.05),  $s$  = standard deviation ( $s_1 = 2.3$ ,  $s_2 = 1.5$ ), and  $\mu_1 - \mu_2$  = mean difference between tested group = 0.8. The calculated sample size was employed 15 specimens per group.

-Preparation of zirconia substructure specimens

One hundred twenty (120) disc specimens of 15 mm in diameter ( $\Phi$ ) and 1 mm thickness were prepared from the pre-shade-A2 partially-sintered 3Y-TZP (Bruxzir, PrismaTik Dentalcraft, Hannover, Germany) block (Table 1) using a diamond-coated disc at a velocity of 700 rounds per minute (rpm) by a water-cool sectioning machine (Isomet-1000, Buehler, Lake Bluff, IL, USA). The waterproof silicon carbide (SiC) abrasive sheets up to no. 5000 were used to grind the zirconia specimens in a wet condition with water using a grinding machine (Ecomet-3, Buehler) at 50 rpm speed. The zirconia specimens were then sintered in a firing furnace (HiTherm, Hint-ELs, Griesheim, Germany) to obtain a final dimension of  $\Phi$  12 mm and thickness of 0.8 mm, owing to 20% shrinkage upon sintering. The zirconia specimens were unintentionally allocated for 8 groups ( $n = 15$ ) for veneering with different ceramics.

-Preparation of veneering ceramics

Different types of the shade-A2 veneering ceramics comprising feldspathic- (Vitablocs; Vm, Vita-Zahnfabrik, Bad Sackingen, Germany), lithium disilicate-based glass- (IPS e.max-CAD; Em, Ivoclar-Vivadent, Schaan, Liechtenstein), zirconia-reinforced glass- (Vita-Suprinity; Vs, Vita-Zahnfabrik), and zirconia-reinforced lithium silicate- (Celtra-Duo; Cd, Dentsply, Hanau-Wolfgang, Germany) ceramic (Table 1) were prepared in disc-shape ( $n = 30$ /ceramic) through a low-velocity diamond saw (Isomet-1000, Buehler) and abraded with SiC abrasive paper up to grit no. 5000 using a water-cool grinding machine (Ecomet-3, Buehler) to obtain the definite dimension of  $\Phi$  12 mm and thickness 0.8 mm. Each kind of ceramics was inadvertently allocated into 2 subclasses ( $n = 15$ ) consistent with CAD-bonded (Cb) or CAD-fused (Cf) to obtain the definite ceramic veneering zirconia comprising 0.8 mm zirconia substructure, 0.04 mm hybridized zone, and 0.8 mm veneering ceramic, determined by a digital caliper (Mitutoyo, Kawasaki, Japan). CAD-bonded hybridized technique

The surfaces of zirconia specimens to be hybridized with the Cb technique were blasted with 50 microns ( $\mu\text{m}$ )  $\text{Al}_2\text{O}_3$  with 2.5 bar pressure in a blasted machine (Vario-basic, Renfert, Hilzingen, Germany) for 15 seconds (sec) by placing a blasting tip 10 mm distance and 45 degrees angulation from the specimen surface

**Table 1:** Material, brand, abbreviation (Abv.), manufacturers, batch number, Young’s modulus, coefficient of thermal expansion (CTE, X10-6 /K) of materials used in this study.

| Material  | Brand          | Abv. | Manufacturer                             | Batch no. | Young’s modulus | CTE      |
|---|----------------|------|--|-----------|-----------------|----------|
| Yttria-stabilized tetragonal zirconia polycrystalline | Bruxzir        | Z    | Prismatik Dentalcraft, Hannover, Germany | B1379641  | 210             | 11       |
| Feldspathic ceramic                                   | Vitablocs      | Vm   | Vita-Zahnfabrik, Bad Sackingen, Germany  | 49470     | 65              | 9.4±1    |
| Lithium disilicate-based glass ceramic                | IPS e.max-CAD  | Em   | Ivoclar-Vivadent, Schaan, Leichtenstein  | V43832    | 95              | 10.1±0.5 |
| Zirconia-reinforced glass ceramic                     | Vita-Suprinity | Vs   | Vita-Zahnfabrik, Bad Sackingen, Germany  | 66418     | 70              | 12.3     |
| Zirconia-reinforced lithium silicate ceramic          | Celtra Duo     | Cd   | Dentsply, Hanau-Wolfgang, Germany        | 18028463  | 70              | 11.8     |

and ultrasonically cleaned in distilled water (Vitasonic-II, Vita-Zahnfabrik) for 15 minutes (min). Then, the hybridized surface of zirconia discs was applied with a zirconia-metal primer (Monobond-Plus, Ivoclar-Vivadent). The surface of veneering ceramics to be hybridized was etched with 5% HF acid (Ivoclar-Vivadent) for 20 sec, sprayed with distilled water, dehydrated in the air, applied with a zirconia-metal primer, coated with thin film resin adhesive (Variolink Esthetic, Ivoclar-Vivadent), then gently condensed against the zirconia specimen using a digital caliper (Mitutoyo) by controlling the resin cement thickness to be exactly 40 µm, and then polymerized with light curing unit (Mini-LED, Acteon, Norfolk, England) for 9 min.

**-CAD-fused hybridized technique**

The surfaces of zirconia specimens to be hybridized with the Cf technique were prepared as previously described before being conjugated with the veneering ceramic discs. The powder-liquid creamy mixture of the fusion glass (e.max CAD Crystall-connect, Ivoclar-Vivadent) was gradually smeared on the whole conjugating side of the veneering ceramics and instantly condensed against the zirconia specimen using digital caliper (Mitutoyo) by controlling the layer of fusion glass to be precisely 40 µm, removed the surplus fusion glass with a micro-brush, and then sintered in the sintering furnace (Programat-P310, Ivoclar-Vivadent) according to the manufacturer’s sintering schedule.

**-Determination of color parameters**

The ColorQuest-XE spectrophotometer (Hunter, Reston, VA, USA) was utilized to determine the color parameters of ceramics veneered zirconia upon different hybridized techniques by setting at D65 illuminant, 100% UV, 10 degrees of observing angle, with a standard wavelength of 380–780 nm. An aperture of 4 mm in Φ was used to facilitate the precise spectrum directly on the specimen to eliminate the edge loss effect during measurement. To provide the analogous location for each sample during the measuring period, the clear repositioning jig was

used to maintain the center of the specimen position. The determinations were made in CIELab (Commission Internationale de l’Eclairage). The L\*, a\*, and b\* parameters were attained from the lightness, red-green, and yellow-blue coordinates, respectively on the white (W) (L<sub>W</sub>\* = 96.70, a<sub>W</sub>\* = 0.10, b<sub>W</sub>\* = 0.20), and black (B) (L<sub>B</sub>\* = 10.40, a<sub>B</sub>\* = 0.40, b<sub>B</sub>\* = 0.60) background. Then, the TP, CR, OP, and ΔE<sub>diff</sub> were computed. The coordinates of the VITA classic shade-A2 (Vita Zahnfabrik) on a white background (L<sub>A2</sub>\* = 65.61, a<sub>A2</sub>\* = -0.50, b<sub>A2</sub>\* = 5.54) were measured and used for determination the amount of color alteration through ΔE<sub>diff</sub> values according to Equation 2 (20), (Fig. 2).

$$E_{diff} = \sqrt{(L_w^* - L_{A2}^*)^2 + (a_w^* - a_{A2}^*)^2 + (b_w^* - b_{A2}^*)^2}$$

**Fig. 2:** Equation 2.

The translucency was determined from the TP values that were calculated from the differences between color determinants on white (W) and black (B) backgrounds, according to Equation 3 (20), (Fig. 3).

$$TP = \sqrt{(L_B^* - L_W^*)^2 + (a_B^* - a_W^*)^2 + (b_B^* - b_W^*)^2}$$

**Fig. 3:** Equation 3.

The contrast was determined from the CR values according to Equations 4 and 5 in which the CR ranged from 0.00 (transparent) to 1.00 (perfectly opaque) (20). In terms of tristimulus color space, Y represents the brightness illuminance; Y<sub>w</sub> and Y<sub>B</sub> are the values of a sample placed on the white and black backgrounds, respectively; and Y<sub>n</sub> is equal to 100, (Figs. 4,5).

$$CR = \frac{Y_B}{Y_W}$$

**Fig. 4:** Equation 4.

$$Y = \left(\frac{L^* + 16}{116}\right)^3 \times Y_n$$

**Fig. 5:** Equation 5.

The opalescence was determined from the OP values that were achieved by using Equation (6) (20), (Fig. 6).

$$OP = \sqrt{(a_B^* - a_W^*)^2 + (b_B^* - b_W^*)^2}$$

Fig. 6: Equation 6.

**-Determining the microstructure**

Three specimens from each group were ultrasonically cleaned in distilled water, dehydrated in the desiccator (Nokko, Nikko, Tokyo, Japan), and coated the surface with gold-palladium in the coating apparatus (K-500X, Emitech, Asford, England) using the current 10 mA for 3 min in the vacuum 130 Torr to evaluate the microstructure. The cross-sectional micrograph was also performed to determine the characteristics of the interface zone of ceramic veneered zirconia, the quality of zirconia-veneering hybridized surface, and the crystalline size of zirconia with scanning electron microscopy (SEM; S-3000N, Hitachi, Osaka, Japan). The Image-J software (U.S. National Institutes of Health, Bethesda, MD, USA) was utilized for measuring the grain size.

**Determining the zirconia phase**

The relative proportions of zirconia crystal phases were assessed with an X-ray diffractometer (XRD, Mini-Flex-2, Rigaku, Tokyo, Japan). The specimens were probed with copper k-alpha (Cu K $\alpha$ ) emission at intervals of two seconds, with the angles of diffraction (2 $\theta$ ) ranging from 20 – 40 degrees (o) with 0.02o stepwise. The phases of zirconia were appraised by cross-reference with the Joint Committee of Powder Diffraction Standards database file (PDF). The analysis of the t- and m-phase proportion was performed by X'Pert-Plus software (Phillips, Almelo, Netherlands). The peaks for the m- and t- phases were identified with PDFs No. 37-1484 and 49-1642, correspondingly. The quantity of t-phase (X<sub>t</sub>) and m-phase (X<sub>m</sub>) to total crystalline phases was computed from the Garvie-Nicholson and Toraya formula as given in Equations 7, 8, 9 (26). The integrated intensities of the m-, and t-phases (I<sub>t</sub> and I<sub>m</sub>) were estimated by matching the complementary peaks with a pseudo-Voigt distribution and considering the area beneath the curves. A correction factor (C) of 1.32 was established from a non-linear adjustment curve of the integrated intensity fractions versus volume fraction to take the impact of yttria doping on the lattice parameters into consideration, (Figs. 7,8,9)

$$x_m = \frac{I_m(111) + I_m(\bar{1}\bar{1}1)}{I_m(111) + I_m(\bar{1}\bar{1}1) + I_t(101)}$$

Fig. 7: Equation 7.

$$x_m = \frac{Cx_m}{1 + (C - 1)x_m}$$

Fig. 8: Equation 8.

$$x_t = 1 - x_m$$

Fig. 9: Equation 9.

**-Statistical analysis**

The data were accomplished for the normality test with the Shapiro-Wilk test, and the homoscedasticity test with Levene's test using IBM SPSS V-28 statistics software (SPSS, Chicago, IL, USA). As the data revealed normal distribution and exhibited homoscedasticity ( $p > 0.05$ ), the two-way analysis of variance (ANOVA) along with Bonferroni multiple comparisons were implemented to detect substantial variations in the color parameters of different CAD/CAM ceramics veneered zirconia upon different hybridized techniques. A statistically significant difference was judged at  $p < 0.05$ . Furthermore, descriptive statistics were employed to evaluate the optical properties, grain size, and relative phases of the zirconia.

**Results**

The mean of TP, CR, OP), and  $\Delta E_{diff}$  together with their standard deviation (SD) of experimental groups were presented (Fig. 10 and Table 2). The VmCf group indicated the highest in both TP and OP values but the lowest in CR values compared to other groups. The VsCf group indicated the lowest in both TP and OP values but the highest in CR values compared to other groups. The highest  $\Delta E_{diff}$  value was revealed in the VsCf group, while the lowest  $\Delta E_{diff}$  value was revealed in the EmCf group, compared to others. ANOVA suggested a statistically significant difference in TP, CR, OP, and  $\Delta E_{diff}$  owing to different veneering ceramics, hybridized techniques, and their interactions ( $p < 0.05$ ) (Table 3). Post-hoc Bonferroni multiple comparison results for each color parameter were presented (Table 4). Regarding the veneering ceramics, Bonferroni multiple comparisons indicated that different veneering ceramics possessed significant differences ( $p < 0.05$ ) in the TP, CR, OP, and  $\Delta E_{diff}$  (Table 4, Fig. 11). The Vm presented significantly higher TP and OP but lower CR than Em, Cd, and VS respectively ( $p < 0.05$ ). A similar  $\Delta E_{diff}$  between Vs and Cd as well as between Vm and Em was demonstrated. Concerning the hybridized techniques, Bonferroni multiple comparisons demonstrated that different hybridized techniques created significant differences ( $p < 0.05$ ) in TP, CR, OP, and  $\Delta E_{diff}$  (Table 4, Fig. 11). The Cb presented significantly higher TP and OP, but lower CR and  $\Delta E_{diff}$  than Cf ( $p < 0.05$ ). The Cb produced a more white, less red-yellow, and more green-blue color appearance in ceramic veneered zirconia than the Cf (Fig. 11). Concerning the interaction of veneering ceramics and hybridized techniques, Bonferroni multiple comparisons indicated that the interaction of hybridized techniques and veneering ceramics created a substantial difference in TP ( $p < 0.05$ ) except for EmCb-CdCb and VsCf-CdCf groups ( $p > 0.05$ ), together with substantial difference in CR ( $p < 0.05$ ) excepting VmCb-VmCf-EmCf, VmCf-EmCf, EmCb-CdCb, and VsCf-CdCf groups ( $p > 0.05$ ), and substantial difference in OP ( $p < 0.05$ ) excepting Vm-

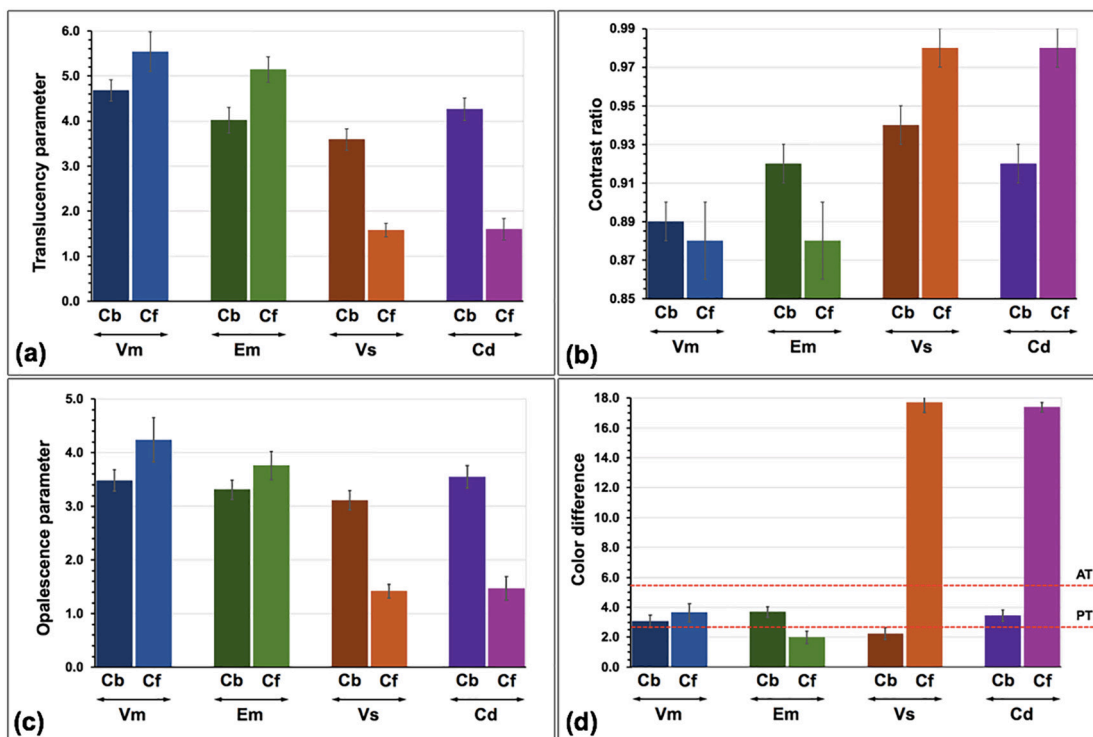


Fig. 10: Translucency parameter (a), contrast ratio (b), opalescence parameter (c), and color difference (d) with perceptible threshold (PT) and acceptable threshold (AT) of Vitabloc (Vm), e.max CAD (Em), Vita Suprinity (Vs), Celtra Duo (Cd) ceramic veneered zirconia (Z) with either CAD-bonded (Cb) or CAD-fused (Cf) technique were shown.

Table 2: Mean, standard deviation (SD) of translucency parameter (TP), contrast ratio (CR), opalescence parameter (OP), color difference ( $\Delta E_{diff}$ ), relative monoclinic (m-), and tetragonal (t-) phase content (wt.%), percentage of phase change (%) and percentage of small (s), medium (m), and large (l) grain size distribution (%) of Vitabloc (Vm), e.max CAD (Em), Vita Suprinity (Vs), Celtra Duo (Cd) ceramic veneered zirconia (Z) with either CAD-bonded (Cb) or CAD-fused (Cf) technique.

| Group | n  | TP        | CR        | OP        | $\Delta E_{diff}$ | Phase (wt%) |      | Phase change (%) | Grain size (%)     |
|-------|----|-----------|-----------|-----------|-------------------|-------------|------|------------------|--------------------|
|       |    | Mean±SD   | Mean±SD   | Mean±SD   |                   | Mean±SD     | m-   |                  |                    |
| VmCb  | 15 | 4.68±0.24 | 0.89±0.01 | 3.48±0.20 | 3.07±0.42         | 12.9        | 87.1 | 8.8              | 41.0 / 57.4 / 1.6  |
| VmCf  | 15 | 5.54±0.44 | 0.88±0.02 | 4.24±0.41 | 3.64±0.62         | 19.6        | 80.4 | 15.6             | 33.3 / 64.8 / 1.9  |
| EmCb  | 15 | 4.02±0.28 | 0.92±0.01 | 3.31±0.18 | 3.68±0.34         | 9.4         | 90.6 | 5.1              | 27.8 / 68.5 / 3.7  |
| EmCf  | 15 | 5.14±0.28 | 0.88±0.02 | 3.76±0.26 | 1.97±0.42         | 15.1        | 84.9 | 11.1             | 30.5 / 64.4 / 5.1  |
| VsCb  | 15 | 3.59±0.24 | 0.94±0.01 | 3.11±0.18 | 2.24±0.39         | 10.7        | 89.3 | 6.5              | 24.5 / 71.7 / 3.8  |
| VsCf  | 15 | 1.58±0.15 | 0.98±0.01 | 1.42±0.13 | 17.69±0.66        | 19.4        | 80.7 | 15.5             | 35.5 / 62.9 / 1.6  |
| CdCb  | 15 | 4.26±0.25 | 0.92±0.01 | 3.55±0.21 | 3.44±0.38         | 9           | 91   | 4.7              | 37.5 / 56.2 / 8.3  |
| CdCf  | 15 | 1.60±0.24 | 0.98±0.01 | 1.47±0.22 | 17.37±0.31        | 18          | 82   | 14.2             | 30.8 / 65.4 / 3.9  |
| Z     | 15 | -         | -         | -         | -                 | 4.5         | 95.5 | -                | 34.0 / 49.1 / 17.0 |

Cb-EmCb-EmCf-CdCb, EmCb-VsCb-CdCb, EmCf-Cd-Cb, and VsCf-CdCf groups ( $p>0.05$ ), and additional substantial differences in  $\Delta E_{diff}$  ( $p<0.05$ ) excepting Vm-Cb-CdCb, VmCf-EmCb-CdCb, EmCf-VsCb, and VsCf-CdCf groups ( $p>0.05$ ) (Fig. 10, Table 4). Concerning the color alteration compared to A2 VITA Classic shade ( $\Delta E_{diff}$ ), the EmCf and VsCb were considered within a PT ( $\Delta E_{diff} \leq 2.6$ ), whereas the remaining groups except

VsCf, and CdCf were considered within an AT ( $\Delta E_{diff} \leq 5.5$ ). However, the impact of Vs and Cd veneering ceramics and hybridized technique on the mean  $\Delta E_{diff}$  values was beyond the AT.

The SEM micrographs displayed dissimilarity in the magnitude of zirconia crystalline particles upon varied veneering ceramics and hybridized techniques. The zirconia crystals were categorized into three groups related

**Table 3:** Two-way ANOVA of (a) translucency parameter (TP), (b) contrast ratio (CR), (c) opalescence parameter (OP), (d) color difference ( $\Delta E_{diff}$ ) of CAD-CAM ceramic veneered zirconia with either CAD-bonded or CAD-fused technique.

| <b>(a) ANOVA of TP upon different factors</b>                        |          |     |          |            |      |
|--|----------|-----|----------|------------|------|
| Source   | SS       | df  | MS       | F          | p    |
| Corrected Model  | 234.785  | 7   | 33.541   | 435.026    | .001 |
| Intercept  | 1734.063 | 1   | 1734.063 | 22490.984  | .001 |
| Ceramic  | 136.667  | 3   | 45.556   | 590.863    | .001 |
| Technique  | 13.637   | 1   | 13.637   | 176.879    | .001 |
| Material * Technique   | 84.480   | 3   | 28.160   | 365.237    | .001 |
| Error  | 8.635    | 112 | .077     |            |      |
| <b>(b) ANOVA of CR upon different factors</b>                        |          |     |          |            |      |
| Corrected Model  | .192     | 7   | .027     | 178.927    | .001 |
| Intercept  | 101.970  | 1   | 101.970  | 666789.191 | .001 |
| Ceramic  | .133     | 3   | .044     | 289.837    | .001 |
| Technique  | .006     | 1   | .006     | 41.810     | .001 |
| Material * Technique   | .052     | 3   | .017     | 113.722    | .001 |
| Error  | .017     | 112 | .000     |            |      |
| <b>(c) ANOVA of OP upon different factors</b>                        |          |     |          |            |      |
| Corrected Model  | 114.011  | 7   | 16.287   | 294.593    | .001 |
| Intercept  | 1109.990 | 1   | 1109.990 | 20076.760  | .001 |
| Ceramic  | 54.153   | 3   | 18.051   | 326.493    | .001 |
| Technique  | 12.427   | 1   | 12.427   | 224.763    | .001 |
| Material * Technique   | 47.432   | 3   | 15.811   | 285.970    | .001 |
| Error  | 6.192    | 112 | .055     |            |      |
| <b>(d) ANOVA <math>\Delta E_{diff}</math> upon different factors</b> |          |     |          |            |      |
| Corrected Model  | 4790.565 | 7   | 684.366  | 3225.173   | .001 |
| Intercept  | 5289.511 | 1   | 5289.511 | 24927.567  | .001 |
| Ceramic  | 1518.467 | 3   | 506.156  | 2385.330   | .001 |
| Technique  | 1496.248 | 1   | 1496.248 | 7051.281   | .001 |
| Material * Technique   | 1775.849 | 3   | 591.950  | 2789.647   | .001 |
| Error  | 23.766   | 112 | .212     |            |      |

NB: SS: sum of squares, df: degree of freedom, MS: mean square, F: F-ratio.

to their grain size: small ( $\leq 0.5 \mu\text{m}$ ), medium ( $0.5 < x \leq 0.7 \mu\text{m}$ ), and large ( $> 0.7 \mu\text{m}$ ), and their relative percentage of grain distribution was presented (Fig. 12a, 13, Table 2). The relative percentage of the grain size distribution for the 3Y-TZP substructure was affected by the veneering ceramics and hybridized techniques (Fig. 12a and Table 2). The microstructures of the zirconia substructure and the zirconia-veneer interface for all investigated groups were shown (Fig. 13 (a-p)). From the cross-sectional core-veneer ceramics, All interfacial junctions among veneering ceramic/resin cement/zirconia substructure were well distinguished (Fig. 13 (i-l)) while the interfacial junction among veneering ceramic/fusion glass/zirconia substructure were well incorporated (Fig. 13 (m-p)). The harmonized conjugations were

noticeable for all interfaces (Fig. 13). The quantity of the zirconia phase was XRD-analyzed as illustrated that the spectral positions of the crystalline phase synchronized with the associating t- and m-phases of zirconia within the firmness of the data (Fig. 12 (b, c), Table 2). The pattern of XRD exhibited a large quantity of t-phase and a tiny quantity of m-phase. The t-phase was identified at the  $2\theta$  degree of  $30.11^\circ$ ,  $34.53^\circ$ , and  $35.09^\circ$ . The m-phases were detected at  $27.79^\circ$  and  $31.12^\circ$ . The XRD data matched the crystallographic patterns signified by the PDF standard. The proportional intensities (wt.%) of m-phases compared to the total quantity of zirconia phases disclosed the alterations in the quantity of the phase conversion from the t→m phase, owing to the influence of veneering ceramics and hybridized techniques (Table

**Table 4:** Post hoc Bonferroni multiple comparisons of (a) translucency parameter (TP), (b) contrast ratio (CR), (c) opalescence parameter (OP), (d) color difference ( $\Delta E_{diff}$ ) of different ceramic (C) including Vitabloc (Vm), e.max CAD (Em), Vita Suprinity (Vs), Celtra Duo (Cd) ceramic veneered zirconia (Z) with either CAD-bonded (Cb) or CAD-fused (Cf) technique (T).

| <b>(a) Post hoc of TP as a function of ceramic, technique, and ceramic*technique interaction</b>                           |    |      |      |      |      |      |      |      |      |      |      |      |      |
|--|----|------|------|------|------|------|------|------|------|------|------|------|------|
| C  | Vm | Em   | Vs   | Cd   | C*T  | VmCb | VmCf | EmCb | EmCf | VsCb | VsCf | CdCb | CdCf |
| Vm   | 1  | .001 | .001 | .001 | VmCb | 1    | .001 | .001 | .001 | .001 | .001 | .001 | .001 |
| Em   |    | 1    | .001 | .001 | VmCf |      | 1    | .001 | .004 | .001 | .001 | .001 | .001 |
| Vs   |    |      | .000 | .001 | EmCb |      |      | 1    | .001 | .002 | .001 | .600 | .001 |
| Cd   |    |      |      | 1    | EmCf |      |      |      | 1    | .001 | .001 | .000 | .001 |
|  |    |      |      |      | VsCb |      |      |      |      | 1    | .001 | .001 | .001 |
| T  | Cb | Cf   |      |      | VsCf |      |      |      |      |      | 1    | .001 | 1    |
| Cb   | 1  | .001 |      |      | CdCb |      |      |      |      |      |      | 1    | .001 |
| Cf   |    | .001 |      |      | CdCf |      |      |      |      |      |      |      | 1    |
| <b>(b) Post hoc of CR as a function of ceramic, technique, and ceramic*technique interaction</b>                           |    |      |      |      |      |      |      |      |      |      |      |      |      |
| C  | Vm | Em   | Vs   | Cd   | C*T  | VmCb | VmCf | EmCb | EmCf | VsCb | VsCf | CdCb | CdCf |
| Vm   | 1  | .001 | .001 | .001 | VmCb | 1    | .150 | .001 | 1    | .001 | .001 | .001 | .001 |
| Em   |    | 1    | .001 | .001 | VmCf |      | 1    | .001 | 1    | .001 | .001 | .001 | .001 |
| Vs   |    |      | 1    | .007 | EmCb |      |      | 1    | .001 | .001 | .001 | 1    | .001 |
| Cd   |    |      |      | 1    | EmCf |      |      |      | 1    | .001 | .001 | .001 | .001 |
|  |    |      |      |      | VsCb |      |      |      |      | 1    | .001 | .001 | .001 |
| T  | Cb | Cf   |      |      | VsCf |      |      |      |      |      | 1    | .001 | 1    |
| Cb   | 1  | .001 |      |      | CdCb |      |      |      |      |      |      | 1    | .001 |
| Cf   |    | 1    |      |      | CdCf |      |      |      |      |      |      |      | 1    |
| <b>(c) Post hoc of OP as a function of ceramic, technique, and ceramic*technique interaction</b>                           |    |      |      |      |      |      |      |      |      |      |      |      |      |
| C  | Vm | Em   | Vs   | Cd   | C*T  | VmCb | VmCf | EmCb | EmCf | VsCb | VsCf | CdCb | CdCf |
| Vm   | 1  | .001 | .001 | .001 | VmCb | 1    | .001 | 1    | .058 | .001 | .001 | 1    | .001 |
| Em   |    | 1    | .001 | .001 | VmCf |      | 1    | .001 | .001 | .001 | .001 | .001 | .001 |
| Vs   |    |      | 1    | .001 | EmCb |      |      | 1    | .001 | .679 | .001 | .176 | .001 |
| Cd   |    |      |      | 1    | EmCf |      |      |      | 1    | .001 | .001 | .484 | .001 |
|  |    |      |      |      | VsCb |      |      |      |      | 1    | .001 | .001 | .001 |
| T  | Cb | Cf   |      |      | VsCf |      |      |      |      |      | 1    | .001 | 1    |
| Cb   | 1  | .001 |      |      | CdCb |      |      |      |      |      |      | 1    | .001 |
| Cf   |    | 1    |      |      | CdCf |      |      |      |      |      |      |      | 1    |
| <b>(d) Post hoc of <math>\Delta E_{diff}</math> as a function of ceramic, technique, and ceramic*technique interaction</b> |    |      |      |      |      |      |      |      |      |      |      |      |      |
| C  | Vm | Em   | Vs   | Cd   | C*T  | VmCb | VmCf | EmCb | EmCf | VsCb | VsCf | CdCb | CdCf |
| Vm   | 1  | .001 | .001 | .001 | VmCb | 1    | .028 | .014 | .001 | .001 | .001 | .946 | .001 |
| Em   |    | 1    | .001 | .001 | VmCf |      | 1    | 1    | .001 | .001 | .001 | 1    | .001 |
| Vs   |    |      | 1    | .003 | EmCb |      |      | 1    | .001 | .001 | .001 | 1    | .001 |
| Cd   |    |      |      | 1    | EmCf |      |      |      | 1    | 1    | .001 | .001 | .001 |
|  |    |      |      |      | VsCb |      |      |      |      | 1    | .001 | .001 | .001 |
| T  | Cb | Cf   |      |      | VsCf |      |      |      |      |      | 1    | .001 | 1    |
| Cb   | 1  | .001 |      |      | CdCb |      |      |      |      |      |      | 1    | .001 |
| Cf   |    | 1    |      |      | CdCf |      |      |      |      |      |      |      | 1    |



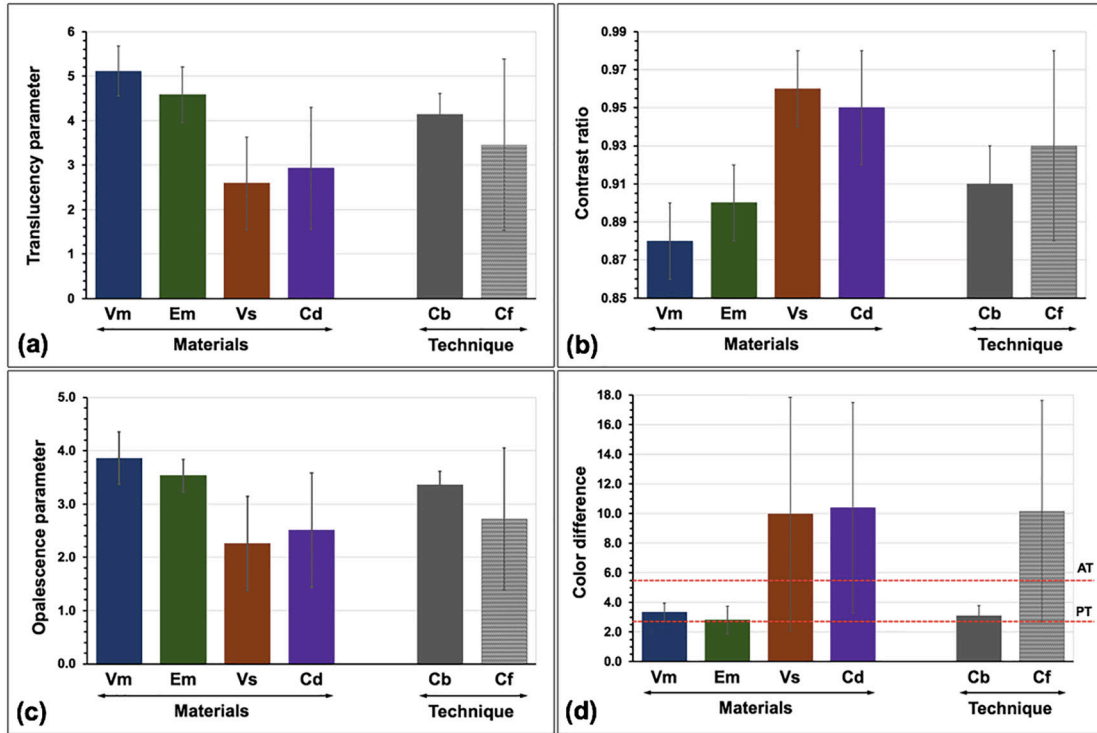


Fig. 11: Influence of materials [Vitabloc (Vm), e.max CAD (Em), Vita Suprinity (Vs), Celtra Duo (Cd) ceramic] veneered zirconia with different hybridization techniques [CAD-bonded (Cb) or CAD-fused] (Cf) on translucency parameter (a), contrast ratio (b), opalescence parameter (c), and color difference (d) with perceptible (PT) and acceptable threshold (AT).

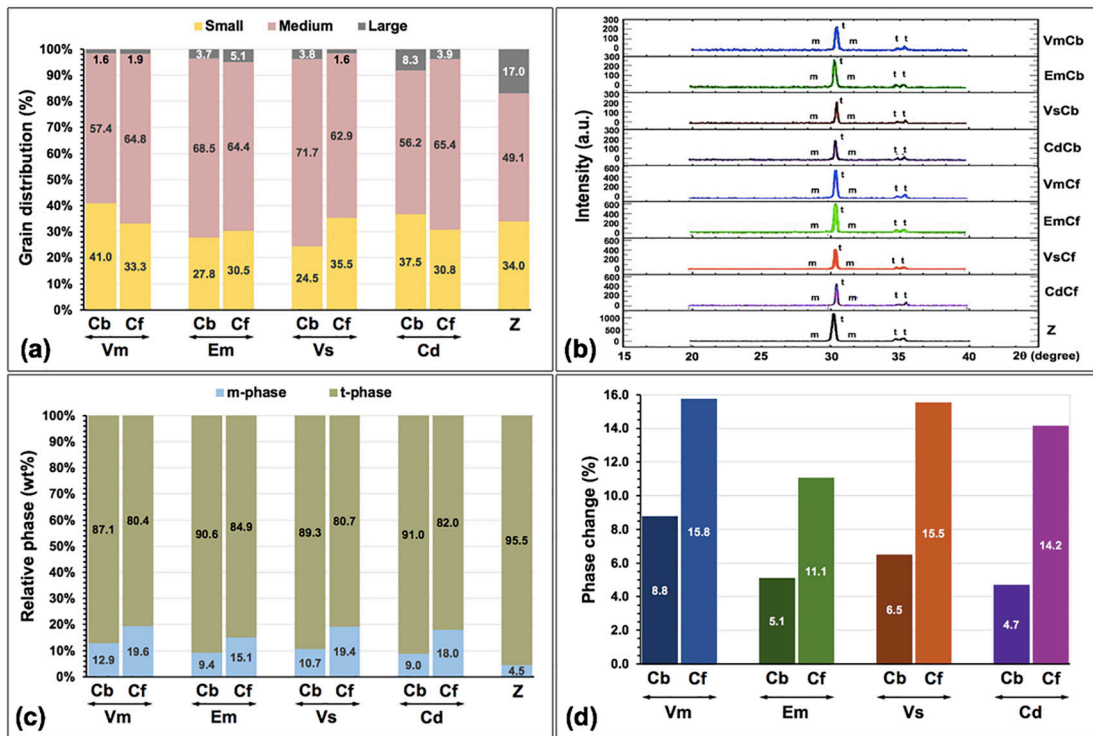
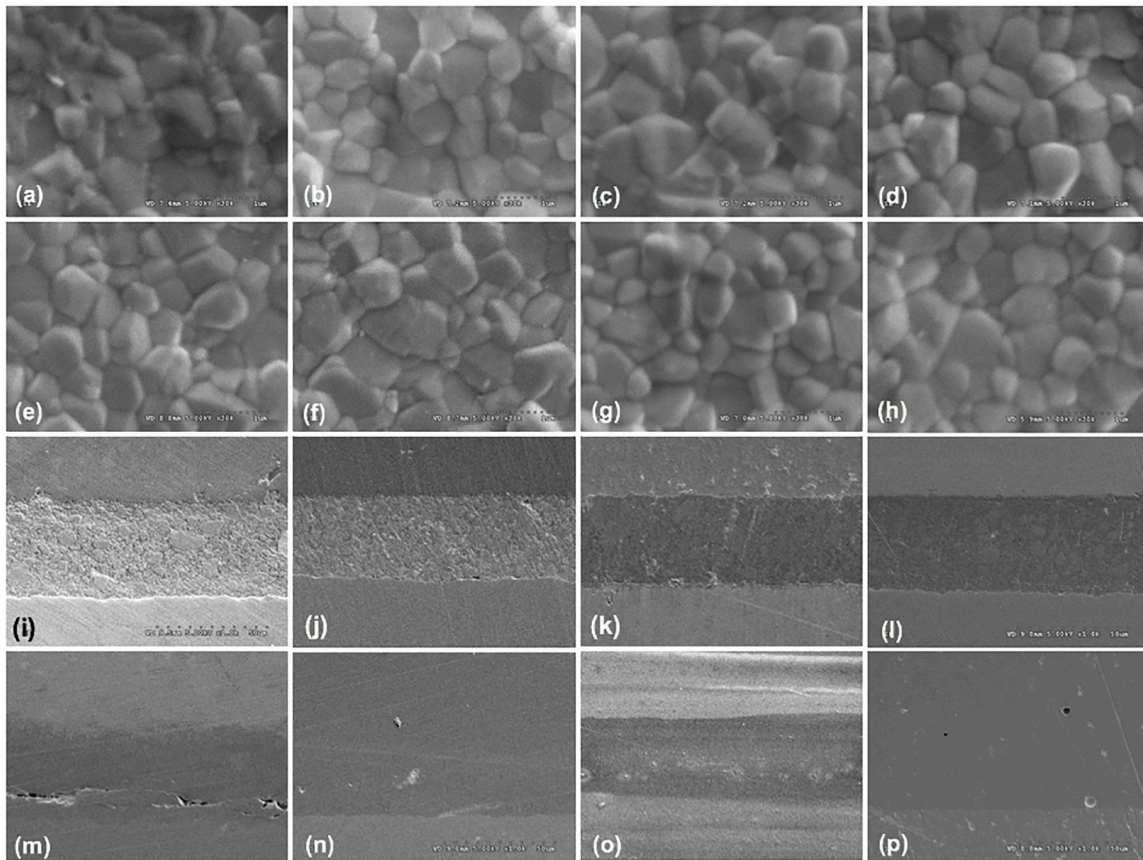


Fig. 12: Grain distribution (a), phase intensity upon x-ray diffraction (b), relative phase of zirconia (c), and percentage of phase change (d) of Vitabloc (Vm), e.max CAD (Em), Vita Suprinity (Vs), Celtra Duo (Cd) ceramic veneered zirconia (Z) with either CAD-bonded (Cb) or CAD-fused (Cf) technique.



**Fig. 13:** Scanning electron microscope photomicrographs of grain size and grain distribution of zirconia at  $\times 30K$  magnification (a-h), and interfacial junction area at  $\times 1000$  magnification (i-p) of Vitabloc (Vm, a, e, i, m), e.max CAD (Em, b, f, j, n), Vita Suprinity (Vs, c, g, k, o), Celtra Duo (Cd, d, h, l, p) ceramic veneered zirconia with either CAD-bonded (Cb, a-d, i-l) or CAD-fused (Cf, e-h, m-p) technique.

2, Fig. 12 (b,c)). The quantity of phase content was associated with the influence of ceramic veneering materials and hybridized techniques. An increase in the relative quantity of  $t \rightarrow m$  phase transformation was greater for CAD-fused hybridized than CAD-bonded hybridized technique (Fig. 12d, Table 2).

## Discussion

To accomplish natural color characteristics restorations, superior translucency, enriched opalescence, and minimized color alteration of ceramic veneered zirconia, different types of ceramic materials veneering zirconia substructures either by CAD-fused or CAD-bonded hybridized techniques were examined in the present study. The substantial statistics differences for whole color parameters including TP, CR, OP, and  $\Delta E_{diff}$  of varied veneering ceramics, with different hybridized techniques, and their interactions were discovered. Hence, all null hypotheses were rejected.

Translucency is a fundamental characteristic of replicating the natural tooth appearance specifically in the esthetic zone, which is defined by TP and CR values of ceramic veneering zirconia (9,18). This current study

indicated substantial impacts on the TP of ceramic veneer zirconia amongst each ceramic material. The Vm is extremely impacted on TP ceramic veneered zirconia, trailed by Em, Cd, and Vs. Contrariwise, Vs supremely influenced on CR of ceramic veneered zirconia, trailed by Cd, Em, and Vm. The study inferred that the feldspathic ceramic provided better translucency to ceramic veneered zirconia than the LS2 glass ceramic, ZLS ceramic, and zirconia-reinforced glass ceramic, respectively. Translucency of ceramics can be affected by the thickness, and crystal microstructure including crystal volume, refractive index, particle size, and number of firing cycles (6, 17). In the present study, TP was altered on account of different veneering ceramics and hybridized techniques. This is possibly related to the varied crystalline contents of each veneering ceramic as well as the reflectance at the interface between the zirconia substructure and veneering ceramics (19). Concerning the hybridized techniques, the Cf technique needs additional firing to fuse veneering ceramics to the zirconia substructure, while Cb does not. For the Vm and Em groups, the Cf technique produced higher TP than the Cb technique. Despite the Vs and Cd groups, the Cf

technique produced lower TP than the Cb technique. The results confirmed a powerful association between Cr and TP; as CR decreases, TP increases, which was supported by other studies (18,27). Conversely, a weak association between direct transmittance and CR was found for CAD/CAM ceramics (27). It was presumed that CR values, measured from diffuse reflectance, are not capable of detection upon minute alterations in light transmission as the materials possess extreme scattering and absorption coefficients (27). The CR was suggested only for ceramics occupied for at least 50% of total transmission (18). As for CR values in the present study, the Cf technique showed lower CR than the Cb technique in the Vm and Em groups, while the Cf technique presented superior CR than the Cb technique in the Vs and Cd groups. These results confirmed that veneering ceramics, hybridized techniques, and their interaction significantly affected the TP and CR of the specimens.

Concerning microstructure, the optical characteristics of ceramic material were influenced by the nature, shape, relative quantity, and distribution of particle size of the crystalline phases and porosity. The Cf technique showed a higher percentage of  $t \rightarrow m$  phase transformation than the Cb technique, this could account for the varied characterization of color in the Cf technique. As for TP values, the highest TP value went to VmCf and the lowest TP value also went to CdCf. As well as for CR values, the highest CR value went to CdCf and the lowest CR value went to VmCf. In the Cb technique, both TP and CR values did not change as much as in the Cf technique. Larger crystal content produces superior fracture strength and, in contrast, can reduce translucence (5). The Vs is a feldspathic ceramic reinforced with sanidine, containing a crystal substance of approximately 30%. The Em is a LS2 glass ceramic, containing a crystal substance of approximately 65%. This confirmed that crystal substance motivates the optical characteristics of ceramics as supported by another study (18). Both Vs and Cd are ZLS ceramics, comprising 10% of zirconia suspended in the lithium silicate glass matrix resulting in 4 times smaller silicate crystals, meaning a higher amount of glass substance and superior translucence than classical LS2 ceramics. The Cd attained higher direct transmittance values than Em (2). Nevertheless, the newest study mentioned that no definite correlation between translucency and contrast since these properties tend to be material-specific (2). Furthermore, the close matching of the refractive index of the crystalline structure and glass matrix is also essential in regulating the translucency and intrinsic appearance of ceramics (18,28). Previous investigations reported that glass-ceramics have an inferior refractive index of 1.5, while zirconia possesses a superior refractive index of 2.2. Less crystal substance coupled with a close refractive index of crystal structure to that of the glass matrix instigates less light scattering

(28). This might be the explanation for the highest TP values of Vm upon veneering zirconia (18). Concerning TP of ceramic material per se used in this study, the highest TP was occupied in Cd ( $17.23 \pm 0.55$ ), followed by Vm ( $15.39 \pm 0.89$ ), Vs ( $14.61 \pm 0.88$ ), Em ( $14.47 \pm 0.75$ ), and Zirconia ( $6.25.47 \pm 40$ ), respectively. However, when veneering ceramics bonded to zirconia with resin cement (TP =  $41.39 \pm 0.51$ ), the VmCb has the highest TP followed by CdCb, EmCb, and VsCb, respectively. In the CAD-fused technique, the order from the highest to lowest TP were VmCf, EmCf, CdCf, and VsCf, respectively. The crystalline volume and refractive index in the present study likewise vary from those of other ceramic systems. Vs and Cd have high crystalline contents; however, the manufacturers claim that the crystalline structure is fine causing these systems to be more translucent. These factors might also have affected the results of the present study.

Opalescence is generated by the scattering effect of the tiny wavelengths of the spectrum of visible light on the small particle sizes of ceramic material, giving the ceramic a bluish appearance in the reflective light and an orange-brown appearance in the transmitted light. To fabricate extremely esthetic ceramic restorations that imitate natural tooth appearance, the ceramics that are capable of generating opalescence ought to be utilized. The OP values of 3.01-7.64 of 1.0 mm thickness of glass ceramics were reported (18), which were greater than the veneering ceramics in this study. Ceramics with superior OP were related to the rising quantities of certain oxides, for example,  $Y_2O_3$ ,  $ZrO_2$ ,  $SnO_2$ , and  $V_2O_5$  (16). Previous study reported that the OP of core material, veneering ceramics, A2-shade ceramic veneered cores were 1.6 - 6.1, 2.0 - 7.1, and 1.3 - 5.0, respectively, which indicated significant influence of types of material on opalescence (29). This study denoted that the OP values of the A2-ceramic veneered zirconia ranged from 1.42 - 4.24, which were in the same range as the previous study (29). Opalescence is associated with translucence, in which the low translucency of the zirconia substructure probably influences the OP value of ceramic veneered zirconia in this study. Concerning hybridized techniques, the Cf technique showed higher OP for Vm and Em veneered zirconia than the Cb technique. Conversely, the Cf technique showed lower OP for Vs and Cd veneered zirconia than the Cb technique. The study confirmed that hybridized techniques, veneering ceramics, and their interaction significantly affected the OP of the specimens. As there was no standard guidance to identify opalescence, the decision concerning the materials being considered as opalescence could not be justified (21). Nevertheless, the OP values in this study were lower than the OP of human enamel ( $22.9 \pm 1.9$ ), thus the ceramics examined in this study probably be classified as non-opalescence.

Regarding color appearance difference between the two subjects is represented by the arithmetic distance difference between  $L^*a^*b^*$  coordinates of two materials ( $\Delta E_{diff}$ ), which may not be detectable by the human eye. The level of visual perception or clinically acceptable color appearance differences varies and is based on an individual basis. However, it was described that  $\Delta E_{diff}$  value as “clinical imperceptible” ( $\Delta E_{diff} < 2.6$ ), “clinical acceptable” ( $\Delta E_{diff} = 2.6 - 5.5$ ), and “clinical unacceptable” ( $\Delta E_{diff} > 5.5$ ) appear to be coherent with the non-expert consideration in clinical practice, which normally related to the patient’s concern (23, 24). It is evident that no matter how the veneering technique is implemented, the  $b^*$  value significantly increases once veneering, indicating the tendency of ceramic veneered zirconia to develop a more yellow appearance. Veneering ceramics materials and hybridized techniques tested in this study tended to demonstrate individual color appearance. This investigation is essential for dentists as well as dental technicians, in that they should be careful when selecting the veneering ceramics to be used with each hybridized technique to the zirconia; the color change of some groups was higher than the clinically acceptable level ( $\Delta E_{diff} > 5.5$ ). Very little data is available on the shade reproduction with different veneering ceramics for zirconia substructure. The differences between the ceramic veneered zirconia substructure and the ceramic veneered metal substructures are mainly related to the difference in the coefficient of thermal expansion. It is hence reasonable to conclude that most of the factors influencing the color appearance of the ceramic veneering metal may affect the ceramic veneering zirconia as well (1,11). In the present study, regardless of the hybridized techniques, color changes occurred after combining veneering ceramic with zirconia substructure. This study also confirmed that the difference in hybridized technique caused a substantial effect on the color appearance of ceramic veneered zirconia restoration, whilst the  $\Delta E_{diff}$  changed. Previous studies stated that the veneering ceramic color was influenced by the ceramic thickness, underlying substrate, and the interaction between them, which supported the result of this study (16, 30). This study confirmed that ceramics veneering zirconia, with the same shade, but from different ceramic types exhibited differences in color appearance, which was consistent with the previous studies (30). The CIELab coordinates for Vita classical shade (VITA Zahnfabrik) show  $L^*$ ,  $a^*$ , and  $b^*$  values for A2 shade equal to 74.0, 1.7, and 19.3 respectively. Compared to the results obtained from this study, the Vita classic shade guide was redder and yellower than the color appearance of the entire experimental groups. The result indicated that upon the use of the claimed shade guide in the process of shade selection for the restoration, the outcome of the shade of the restoration is certainly not the same as expected.

Thus, the clinician should keep in mind that the final shade of the restoration is almost always different from the selected shade, due to the different materials used to fabricate restoration and the technique in combination, as discovered in this study.

## Conclusions

The study herein revealed that types of veneering ceramic, hybridized technique, and their interaction affected the color characteristics of ceramic veneered zirconia. Veneering zirconia with either Vm or Em provided greater translucency and opalescence, but less contrast and color alteration than veneered with Vs or Cd. Cf hybridized technique yielded less translucency and opalescence, but higher contrast and color alteration to ceramic veneered zirconia than Cb hybridized technique. Zirconia veneering with either Vm or Em and with either Cb or Cf hybridized technique, appeared to produce better translucence and opalescence, with less contrast and color alteration than veneering with either Vs or Cd and with either Cb or Cf hybridized technique. However, the color alteration for different ceramics veneering zirconia, with different hybridized techniques remained within an acceptable limit, except for both Vs and Cd upon the Cf hybridized technique.

### -Clinical implications

To produce CAD-CAM ceramic veneered zirconia restoration with enhanced translucency, opalescence, and optimal contrast and color alteration, it is recommended to veneer the zirconia substructure with either feldspathic or lithium disilicate-based glass ceramic compared to zirconia reinforced glass ceramic and zirconia reinforced lithium silicate ceramic. Ceramic veneering zirconia with a CAD-bonded hybridized technique produces better translucency, opalescence, and less contrast and color alteration than veneering with a CAD-fused hybridized technique. Nevertheless, it could be deemed acceptable for color alteration, meaning acceptable color stability of zirconia to be veneered with any veneering ceramic through either CAD-fused or CAD-bonded technique, except only zirconia-reinforced glass ceramic and zirconia reinforced lithium silicate ceramic need to be veneered by CAD-bonded hybridized technique.

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### Institutional Review Board Statement

The study was approved by (Grant No. RTG27062561).

### Data Availability Statement

The datasets used and/or analyzed during the current study are available from the corresponding author.

### Author Contributions

Not specified.

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None.

**Conflict of interest**

The authors declare that they have no conflict of interest.

**References**

1. Vichi A, Louca C, Corciolani G, Ferrari M. Color related to ceramic and zirconia restorations: a review. *Dent Mater.* 2011;27(1):97-108.
2. Awad D, Stawarczyk B, Liebermann A, Ilie N. Translucency of esthetic dental restorative CAD/CAM materials and composite resins with respect to thickness and surface roughness. *J Prosthet Dent.* 2015;113(6):534-40.
3. Traini T, Sinjari B, Pascetta R, Serafini N, Perfetti G, Trisi P, et al. The zirconia-reinforced lithium silicate ceramic: lights and shadows of a new material. *Dent Mater J.* 2016;35(5):748-55.
4. Bachhav VC, Aras MA. Zirconia-based fixed partial dentures: a clinical review. *Quintessence Int.* 2011;42(2):173-82.
5. Church TD, Jessup JP, Guillory VL, Vandewalle KS. Translucency and strength of high-translucency monolithic zirconium oxide materials. *Gen Dent.* 2017;65(1):48-52.
6. Luo XP, Zhang L. Effect of veneering techniques on color and translucency of Y-TZP. *J Prosthodont.* 2010;19(6):465-70.
7. Alghazzawi TF, Lemons J, Liu PR, Essig ME, Janowski GM. Evaluation of the optical properties of CAD-CAM generated yttria-stabilized zirconia and glass-ceramic laminate veneers. *J Prosthet Dent.* 2012;107(5):300-8.
8. Zhang L, Luo X, Shi Y. Effect of veneering technologies on color and translucency of Y2O3 stabilized tetragonal zirconia polycrystals all-ceramic restorations. *Chinese J Stomatol.* 2008;43(3):178-81.
9. Zhang Y. Making yttria-stabilized tetragonal zirconia translucent. *Dent Mater.* 2014;30(10):1195-203.
10. Larsson C, Wennerberg A. The clinical success of zirconia-based crowns: a systematic review. *Int J Prosthodont.* 2014;27(1):33-43.
11. Celik G, Uludag B, Usumez A, Sahin V, Ozturk O, Goktug G. The effect of repeated firings on the color of an all-ceramic system with two different veneering porcelain shades. *J Prosthet Dent.* 2008;99(3):203-8.
12. Jeong ID, Bae SY, Kim DY, Kim JH, Kim WC. Translucency of zirconia-based pressable ceramics with different core and veneer thicknesses. *J Prosthet Dent.* 2016;115(6):768-72.
13. Schmitter M, Mueller D, Rues S. Chipping behaviour of all-ceramic crowns with zirconia framework and CAD/CAM manufactured veneer. *J Dent.* 2012;40(2):154-62.
14. Elsaka SE, Elnaghy AM. Mechanical properties of zirconia reinforced lithium silicate glass-ceramic. *Dent Mater.* 2016;32(7):908-14.
15. Baldissara P, Llukacej A, Ciocca L, Valandro FL, Scotti R. Translucency of zirconia copings made with different CAD/CAM systems. *J Prosthet Dent.* 2010;104(1):6-12.
16. Turgut S, Bagis B. Effect of resin cement and ceramic thickness on final color of laminate veneers: an in vitro study. *J Prosthet Dent.* 2013;109(3):179-86.
17. Malkondu O, Tinastepe N, Kazazoglu E. Influence of type of cement on the color and translucency of monolithic zirconia. *J Prosthet Dent.* 2016;116(6):902-8.
18. Della Bona A, Nogueira AD, Pecho OE. Optical properties of CAD-CAM ceramic systems. *J Dent.* 2014;42(9):1202-9.
19. Heffernan MJ, Aquilino SA, Diaz-Arnold AM, Haselton DR, Stanford CM, Vargas MA. Relative translucency of six all-ceramic systems. Part II: core and veneer materials. *J Prosthet Dent.* 2002;88(1):10-5.
20. Bona A, Nogueira A, Pecho O. Optical properties of CAD-CAM ceramic systems. *J Dent.* 2014;42(9):1202-9.
21. Cho MS, Yu B, Lee YK. Opalescence of all-ceramic core and veneer materials. *Dent Mater.* 2009;25(6):695-702.
22. Lee YK, Yu B. Measurement of opalescence of tooth enamel. *J Dent.* 2007;35(8):690-4.
23. Juntavee N, Attashu S. Effect of sintering process on color parameters of nano-sized yttria partially stabilized tetragonal monolithic zirconia. *J Clin Exp Dent.* 2018;10(8):e794-e804.
24. Alghazali N, Burnside G, Moallem M, Smith P, Preston A, Jarad FD. Assessment of perceptibility and acceptability of color difference of denture teeth. *J Dent.* 2012;40:e10-e7.
25. Sailer I, Holderegger C, Jung RE, Suter A, Thievent B, Pietrobon N, et al. Clinical study of the color stability of veneering ceramics for zirconia frameworks. *Int J Prosthodont.* 2007;20(3):263-9.
26. Stefanic G, Grzeta B, Popović S, Musić S. In situ Phase analysis of the thermal decomposition products of zirconium salts. *Croatica Chemica Acta.* 1999;72(2):395-412.
27. Nogueira AD, Della Bona A. The effect of a coupling medium on color and translucency of CAD-CAM ceramics. *J Dent.* 2013;41(Suppl 3):e18-e23.
28. Stawarczyk B, Emslander A, Roos M, Sener B, Noack F, Keul C. Zirconia ceramics, their contrast ratio and grain size depending on sintering parameters. *Dent Mater J.* 2014;33(5):591-8.
29. Shiraiishi T, Wood DJ, Shinozaki N, van Noort R. Optical properties of base dentin ceramics for all-ceramic restorations. *Dent Mater.* 2011;27(2):165-72.
30. Oh SH, Kim SG. Effect of abutment shade, ceramic thickness, and coping type on the final shade of zirconia all-ceramic restorations: in vitro study of color masking ability. *J Adv Prosthodont.* 2015;7(5):368-74.